

Validity of a low-cost friction encoder for measuring velocity, force and power in flywheel exercise devices

AUTHORS: Víctor Illera-Domínguez^{1,2}, Bruno Fernández-Valdés², Jose Gisbert-Orozco¹, Carlos Ramirez-Lopez^{3,4}, Sergi Nuell^{1,2}, Jacob González^{1,5}, Jonathon Weakley^{3,6}

¹ Institut Nacional d'Educació Física de Catalunya (INEFC), Universitat de Barcelona, Barcelona, Spain

² Tecnocampus, Department of Health Sciences, Pompeu Fabra University, Mataró, Spain

³ Carnegie Applied Rugby Research (CARR) centre, Institute for Sport, Physical Activity and Leisure, Carnegie School of Sport, Leeds Beckett University, Leeds, United Kingdom

⁴ Scottish Rugby Union, Murrayfield Stadium, Edinburgh, United Kingdom

⁵ Futbol Club Barcelona (FCB), Barcelona, Spain

⁶ School of behavioral and health sciences, Australian Catholic University, Brisbane, Australia

ABSTRACT: The purpose of this study was to investigate the validity of a low-cost friction encoder against a criterion measure (strain gauge combined with a linear encoder) for assessing velocity, force and power in flywheel exercise devices. Ten young and physically active volunteers performed two sets of 14 maximal squats on a flywheel inertial device (YoYo Technology, Stockholm, Sweden) with five minutes rest between each set. Two different resistances were used (0.075 kg · m² for the first set; 0.025 kg · m² for the second). Mean velocity (V_{rep}), force (F_{rep}) and power (P_{rep}) for each repetition were assessed simultaneously via a friction encoder (ChronoJump, Barcelona, Spain), and with a strain gauge combined with a linear encoder (MuscleLab 6000, Ergotest Technology, Porsgrunn, Norway). Results are displayed as (Mean [CI 90%]). Compared to criterion measures, mean bias for the practical measures of V_{rep} , F_{rep} and P_{rep} were moderate (-0.95 [-0.99 to -0.92]), small (0.53 [0.50 to 0.56]) and moderate (-0.68 [-0.71 to -0.65]) respectively. The typical error of estimate (TEE) was small for all three parameters; V_{rep} (0.23 [0.20 to 0.25]), F_{rep} (0.20 [0.18 to 0.22]) and P_{rep} (0.18 [0.16 to 0.20]). Correlations with MuscleLab were nearly perfect for all measures in all load configurations. Based on these findings, the friction encoder provides valid measures of velocity, force and power in flywheel exercise devices. However, as error did exist between measures, the same testing protocol should be used when assessing changes in these parameters over time, or when aiming to perform inter-individual comparisons.

CITATION: Illera-Domínguez V, Fernández-Valdés B, Gisbert-Orozco J. Validity of a low-cost friction encoder for measuring velocity, force and power in flywheel exercise devices. *Biol Sport*. 2023;40(3):805–811.

Received: 2022-06-09; Reviewed: 2022-07-22; Re-submitted: 2022-09-08; Accepted: 2022-09-15; Published: 2022-11-18

INTRODUCTION

Quantifying training loads is an important consideration for sports scientists and practitioners. Accurate quantification can ensure that training is both appropriate and meets the programme requirements [1]. Furthermore, this information is essential for informing decision making so that negative training outcomes (e.g. overtraining, illness, and maladaptation) can be avoided [2]. For this reason, tools that are used to quantify training need to be valid so that accurate training information can be gathered. This is relevant for all training methods, including resistance training.

Traditional resistance training methods (e.g. gravity-dependent loads such as dumbbells and barbells), are often quantified through the mass and number of repetitions completed (e.g. volume load) [3]. However, alternative methods of resistance training, such as flywheel training, can be more challenging to quantify as they do not have a constant external load and rely on athletes overcoming inertia to accelerate or decelerate the mass of the wheels (i.e. isoinertial

training) [4]. Despite these practical difficulties in quantifying training loads, the popularity of flywheel devices has grown in recent times due to their ability to induce positive adaptations in strength, power, and velocity [5]. Furthermore, their ability to easily apply eccentric overload (i.e. brief episodes in which eccentric output is higher compared to the concentric output) may provide benefits that can be difficult to achieve using traditional training methods [5, 6]. For an extended description of the eccentric overload concept, relevance, and the available ways for its quantification the reader is referred to a recent review on the topic [7].

Several laboratory technologies can be used for quantifying movement velocity (e.g. linear encoders or optical motion sensing systems) and force (e.g. force plates or strain gauges) during isoinertial exercises [8–12]. However, since some of the aforementioned tools are expensive laboratory-based pieces of equipment, these are not viable options for most practitioners. Another limitation is that

Corresponding author:

Bruno Fernández-Valdés

TecnoCampus Mataró-Maresme
Passatge d'Adolf Comerón, 10
08302 Mataró (Barcelona)
Spain
Tel.: + 34 93 169 65 00
E-mail: bfernandez-valdes@tecnocampus.cat

ORCID:

Víctor Illera-Domínguez
0000-0002-3521-2332

Bruno Fernández-Valdés
0000-0003-3232-1178

Jose Gisbert-Orozco
0000-0003-0253-3073

Carlos Ramirez-Lopez
0000-0003-1605-3484

Sergi Nuell
0000-0002-0772-8534

Jonathon Weakley
0000-0001-7892-4885

Key words:

Iso-inertial
Monitoring
Resistance Training
Feedback

power measurement requires the combination of at least two sensors for being calculated as the product of force and velocity [9, 10]. Therefore, the necessary set-up of sensors and wires may not be convenient in day-to-day training.

To facilitate the quantification of isoinertial training loads, monitoring devices known as axis rotary encoders have been developed. These kinetic sensors are welded to the axis to track flywheel angular velocity and relate these data to a constant moment of inertia to estimate applied force and power in real time. Recent works have demonstrated that flywheel resistance training can be accurately quantified through the use of these sensors [9, 10, 13]. However, one of the biggest limitations is that axis rotary encoders have to be installed by the manufacturer through industrial mechanization of the pieces. In this sense, the encoder is specific to the isoinertial training system and can not be disarmed and used with different devices.

To circumnavigate this issue, rotary friction encoders have been developed. These sensors are not specific or welded to a unique isoinertial training system, but instead can be adapted and used to monitor different isoinertial machines. This is a very relevant feature, as it allows for monitoring existing non-sensorized equipment in a few minutes. Rotary friction encoders consist of a wheel which has to be tightly attached to the rotating flywheel. Due to friction between the two surfaces, the encoder shares the same linear velocity with the point where it is installed. Force, power, and velocity that is being produced by the athlete during training are calculated in real time from the encoder measures of rotational velocity, using given configuration parameters such as the moment of inertia of the wheel, additional masses, and diameters of the pieces (e.g. axis). Therefore, by introducing these set-up parameters in the software, the sensor can be adapted to different inertial training systems.

Although the practicality and relevance of rotary friction encoders is evident, their criterion validity has not been assessed, so the accuracy of the provided feedback is still unknown. Thus, the aim of this study was to assess the criterion validity of force, power, and velocity outputs that are calculated at two different isoinertial loads from a rotary friction encoder.

MATERIALS AND METHODS

Experimental Approach to the Problem

The study was designed to evaluate the criterion validity of force, velocity and power values measured with a commonly used low-cost friction encoder (Chronojump, Barcelona, Spain). In order to do so, half-squats performed on a flywheel with two different isoinertial loads ($0.075 \text{ kg} \cdot \text{m}^2$ and $0.025 \text{ kg} \cdot \text{m}^2$) were simultaneously monitored using (I, practical measure) a friction encoder attached at a known diameter of the flywheel, and (II, criterion measure) a strain gauge combined with a linear encoder attached to the harness. The level of agreement between force, velocity and power obtained from both methods was assessed.

Subjects

Ten physically active male and female volunteers (age 27.9 ± 4.9 years, body mass 70.6 ± 11.9 kg, height 174.5 ± 8.3 cm) were recruited to take part in this study. Subjects were free of injury and illness during data collection. All subjects had previously trained with the exercise device and were familiar with the testing protocol and isoinertial loads used. All experimental procedures were approved by the Catalan Sports Council (Generalitat de Catalunya) ethics committee, and written consent was provided by all subjects before study initiation.

Procedures

An exercise protocol consisting of maximal voluntary concentric-eccentric bilateral half-squats was performed on a “YoYo squat” flywheel device (YoYo Technology, Stockholm, Sweden). An extended description of the exercise can be found elsewhere [14]. Subjects performed two sets of the exercise, consisting of three sub-maximal reps to accelerate the disk, followed by 14 repetitions with maximal intent. In order to test the validity of the friction encoder in different load configurations, two different resistances were used: The moment of inertia was $0.075 \text{ kg} \cdot \text{m}^2$ for one set and $0.025 \text{ kg} \cdot \text{m}^2$ for the other. These load configurations were selected because they are commonly used both in research and in the professional practice [6, 7] and have previously been described as high and low isoinertial load configurations for the squat [15]. The order that subjects completed these different isoinertial loads were randomized by a coin toss. Mean velocity (V_{rep}), force (F_{rep}) and power (P_{rep}) for each repetition were assessed simultaneously via a friction encoder, and strain gauge combined with a linear encoder.

Criterion measures of velocity, force and power were assessed by a strain gauge synchronized with a linear encoder using a Muscle-Lab 6000 (Ergotest Technology, Porsgrunn, Norway). This device has been used before as a measurement reference system in inertial training [10, 12]. The strain gauge (accuracy 63 g, sampling rate: 200 Hz) was attached between the strap of the flywheel and the vest; and the linear encoder (accuracy 0.019 mm; sampling rate 200 Hz) was placed on the flywheel device and attached to the vest, forming a perpendicular angle with the floor (Figure 1).

The friction encoder (Chronojump, Barcelona, Spain), (accuracy 1 mm, sampling rate 1000 Hz) was tightly attached at a known diameter of the flywheel, sharing the same linear velocity (Figure 1). The set-up parameters such as disk inertia, axis diameter, and the volunteer's body mass were entered into the associated Chronojump software (v1.8.1–95) to compute the practical measures of velocity, force and power in real time. Chronojump is an open-code software, and a complete repository of the code and formulas used can be found online [16].

As previously introduced, axis diameter is an essential parameter for computing kinematic variables from the friction encoder, because it determines the point at which the strap exerts unwinding force, and therefore modifies the moment arm and torque. In the

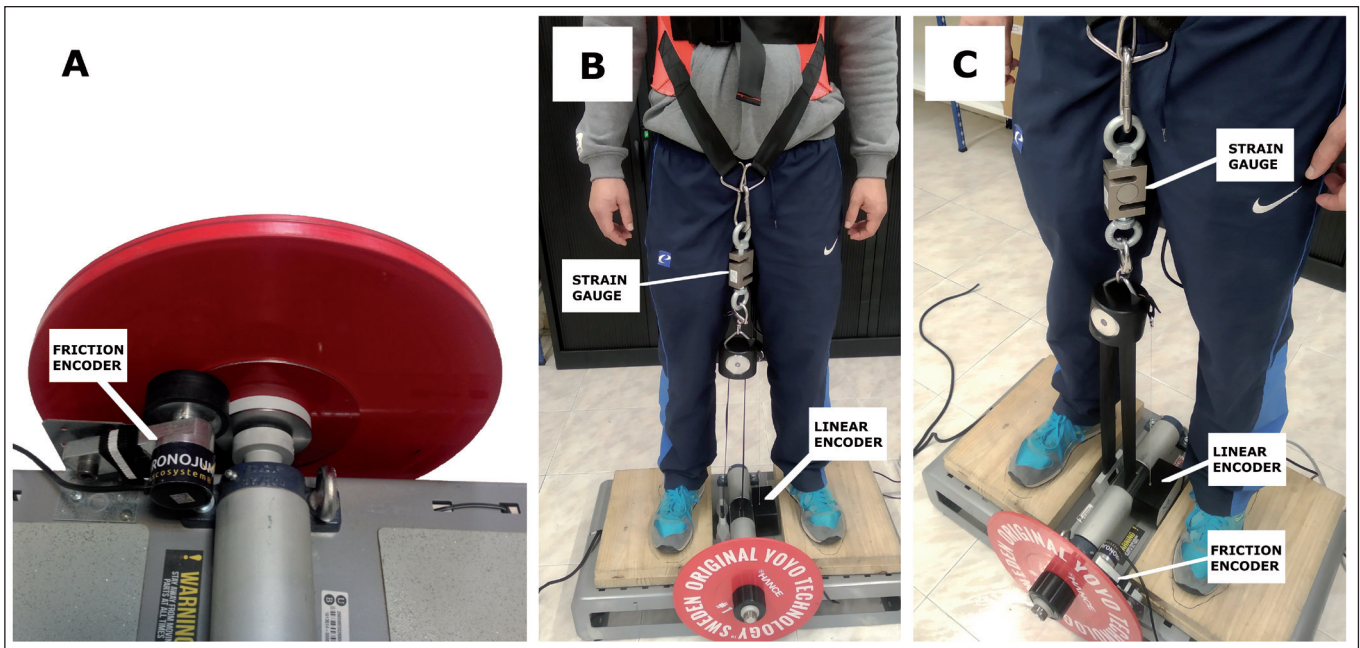


FIG. 1. Disposition of the different sensors used in the study. (A) The friction encoder was tightly attached at a known diameter of the flywheel, sharing the same linear velocity. (B) The strain gauge was attached between the strap of the flywheel and the vest, and the linear encoder was placed on the flywheel device and attached to the vest, forming a perpendicular angle with the floor. (C) General view of the setup.

TABLE 1. Comparison of V_{rep} , F_{rep} and P_{rep} between MuscleLab and Chronojump at high ($0.075 \text{ kg} \cdot \text{m}^2$) and low ($0.025 \text{ kg} \cdot \text{m}^2$) load configurations, and the total pooled data. Data is presented as mean values (\pm standard deviation (SD)) and mean bias, typical error of the estimate and Pearson correlation coefficient, all with 90% confidence limits.

Load	Variable	Criterion Measure	Practical Measure	Bias	TEE	Correlation
High ($0.075 \text{ kg} \cdot \text{m}^2$)	V_{rep}	MuscleLab $0.37 \pm 0.06 \text{ m/s}$	Chronojump $0.28 \pm 0.04 \text{ m/s}$	-1.44 [-1.49 to -1.39] (large)	0.26 [0.23 to 0.31] (small)	0.97 [0.96 to 0.97] (nearly perfect)
	F_{rep}	MuscleLab $1090.0 \pm 306.1 \text{ N}$	Chronojump $1294.6 \pm 353.2 \text{ N}$	0.67 [0.63 to 0.70] (moderate)	0.18 [0.15 to 0.20] (small)	0.98 [0.98 to 0.99] (nearly perfect)
	P_{rep}	MuscleLab $414.2 \pm 160.6 \text{ W}$	Chronojump $312.4 \pm 118.2 \text{ W}$	-0.63 [-0.67 to -0.59] (moderate)	0.13 [0.12 to 0.15] (small)	0.99 [0.99 to 0.99] (nearly perfect)
Low ($0.025 \text{ kg} \cdot \text{m}^2$)	V_{rep}	MuscleLab $0.55 \pm 0.10 \text{ m/s}$	Chronojump $0.41 \pm 0.07 \text{ m/s}$	-1.48 [-1.54 to -1.42] (large)	0.38 [0.33 to 0.44] (moderate)	0.93 [0.91 to 0.95] (nearly perfect)
	F_{rep}	MuscleLab $830.1 \pm 222.3 \text{ N}$	Chronojump $942.0 \pm 243.9 \text{ N}$	0.50 [0.46 to 0.54] (small)	0.27 [0.24 to 0.32] (small)	0.96 [0.95 to 0.97] (nearly perfect)
	P_{rep}	MuscleLab $478.0 \pm 177.9 \text{ W}$	Chronojump $344.8 \pm 126.5 \text{ W}$	-0.75 [-0.80 to -0.70] (moderate)	0.20 [0.17 to 0.23] (small)	0.98 [0.97 to 0.99] (nearly perfect)
Total	V_{rep}	MuscleLab $0.46 \pm 0.13 \text{ m/s}$	Chronojump $0.34 \pm 0.09 \text{ m/s}$	-0.95 [-0.99 to -0.92] (moderate)	0.23 [0.20 to 0.25] (small)	0.98 [0.97 to 0.98] (nearly perfect)
	F_{rep}	MuscleLab $960.1 \pm 297.1 \text{ N}$	Chronojump $1118.3 \pm 350.7 \text{ N}$	0.53 [0.50 to 0.56] (small)	0.20 [0.18 to 0.22] (small)	0.98 [0.98 to 0.98] (nearly perfect)
	P_{rep}	MuscleLab $446.1 \pm 172.2 \text{ W}$	Chronojump $328.6 \pm 123.3 \text{ W}$	-0.68 [-0.71 to -0.65] (moderate)	0.18 [0.16 to 0.20] (small)	0.98 [0.98 to 0.99] (nearly perfect)

V_{rep} = Mean repetition velocity. F_{rep} = Mean repetition force. P_{rep} = Mean repetition power

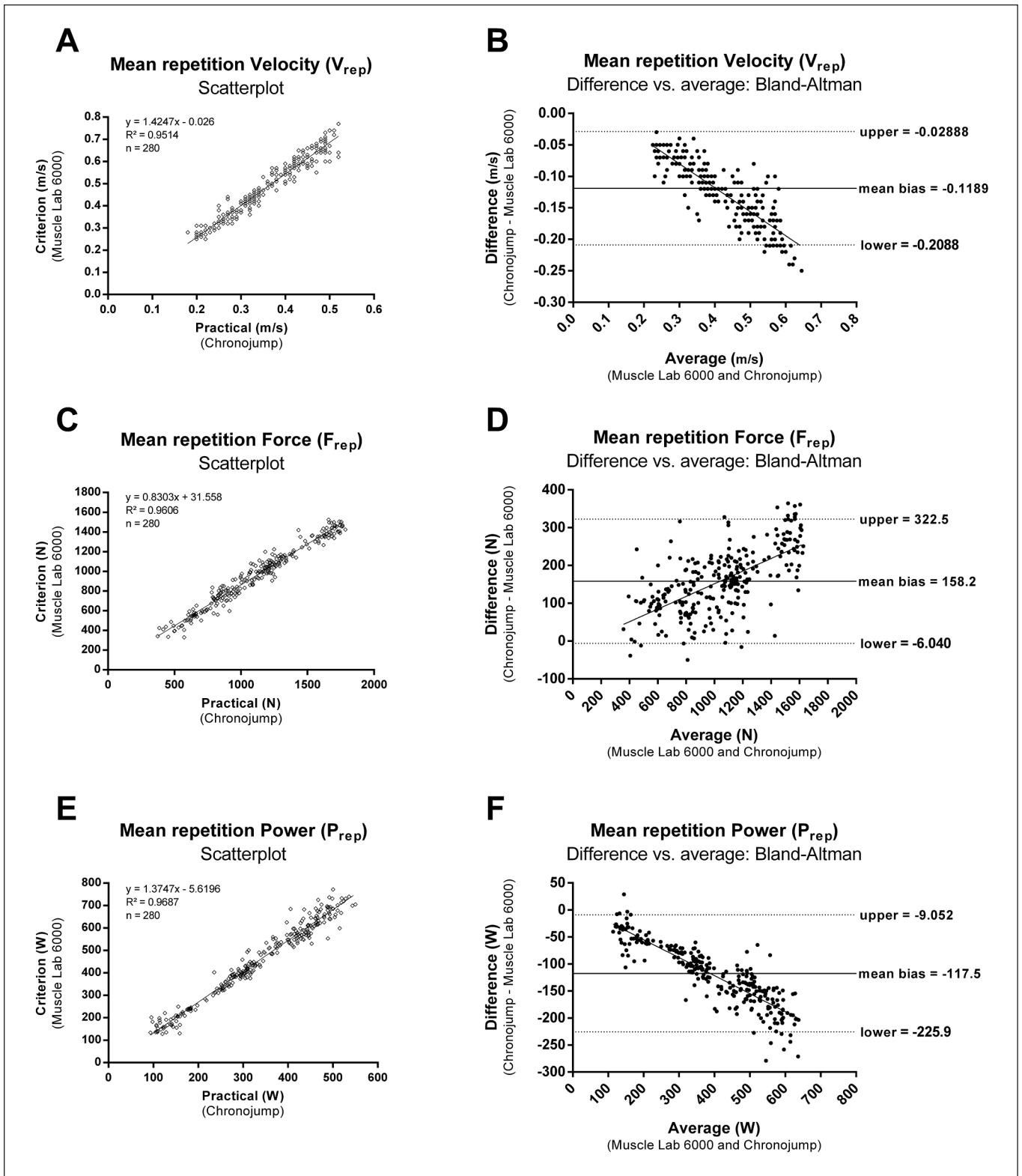


FIG. 2. Scatterplots showing the agreement between the criterion and practical measures V_{rep} (A), F_{rep} (C) and P_{rep} (E). Bland-Altman plots for V_{rep} (B), F_{rep} (D) and P_{rep} (F). The solid horizontal line within the graphs represents the mean bias. The broken horizontal lines represent the upper and lower 95% limits of agreement. The regression lines of the scattered points are shown to investigate the homoscedasticity of the errors.

particular training device used in this study, the diameter is slightly variable across the repetition, given that the strap rolls over on itself increasing the diameter. For this reason, the mean diameter value was used for the estimations.

Raw data from each of the 14 high-intensity repetitions of each set were averaged to compute repetition mean velocity (V_{rep}), force (F_{rep}) and power (P_{rep}), for both measuring systems.

Statistical Analysis

Agreement between the criterion measures (MuscleLab) and the practical measures (Chronojump) of V_{rep} , F_{rep} and P_{rep} was assessed using an excel spreadsheet for analysis of validity [17] designed to calculate the mean bias, typical error of the estimate (TEE) and Pearson correlation coefficient, all with 90% confidence limits. The standardised mean bias was rated as trivial (≤ 0.19), small (0.2–0.59), moderate (0.6–1.19) or large (1.2–1.99) [17]. The standardised typical error was rated as trivial (< 0.1), small (0.1–0.29), moderate (0.3–0.59) or large (> 0.59) [17]. The magnitude of correlation was rated as trivial (< 0.1), small (0.1–0.29), moderate (0.3–0.49), large (0.5–0.69), very large (0.7–0.89) or nearly perfect (0.9–0.99) [17]. Additionally, Bland–Altman plots were used to graphically complement the differences between the two systems [18].

RESULTS

When compared to criterion measures, mean bias for the practical measures of V_{rep} , F_{rep} and P_{rep} were moderate, small and moderate respectively. The TEE was small for all three parameters (Table 1). Correlations with MuscleLab were nearly perfect for all measures in all load configurations (Table 1).

The regression equations to estimate the criterion measures from the practical measures fitted well with data (Figure 2A, 2C, 2E) and are presented as follows:

$$Y = \text{intercept} + (\text{slope} \cdot X)$$

where Y is the estimated criterion measure and X is the practical measure.

The regression equation of V_{rep} is:

$$Y = -0.026 + (1.4247 \cdot X)$$

The regression equation of F_{rep} is:

$$Y = 31.558 + (0.8303 \cdot X)$$

The regression equation of P_{rep} is:

$$Y = -5.6196 + (1.3747 \cdot X)$$

The Bland–Altman plots visually showed the differences between the two systems for the measurement of V_{rep} , F_{rep} and P_{rep} (Figure 2B, 2D, 2F).

DISCUSSION

The primary finding of this study demonstrates acceptable levels of agreement between a low-cost, easy and versatile method (Chronojump friction encoder) and criterion measure (strain gauge combined with a linear encoder) for the assessment of velocity, force and power in a flywheel exercise device with different isoinertial loads.

The friction encoder demonstrated small to moderate TEE and nearly perfect relationships across all kinetic and kinematic variables at both isoinertial loads. However, small to large bias was demonstrated, which should be acknowledged when implemented in training and future research. Considering these findings, the Chronojump friction encoder is a valid tool for the quantification of training loads when completing flywheel resistance training.

The monitoring of kinetic and kinematic variables is an important consideration for the accurate quantification of resistance training intensity. Furthermore, these external stimuli provide a greater understanding of the internal and fatigue responses that determine muscular adaptations [19]. Small to moderate TEE for all were found, which suggests that the Chronojump device can adequately provide repetition information during exercise. This will not only be of use to practitioners and scientists but also athletes, as this device can provide live augmented feedback that may enhance psychological traits during resistance training and subsequent physical adaptations [20]. However, the small to large bias that was present suggests that findings may be smaller or greater depending on the variable assessed (i.e. velocity and power may be consistently lower and force consistently higher than actual values). Thus, it is advised that, due to the lowest TEE and bias observed, power outputs are monitored in the detection of changes in neuromuscular performance.

Differences between measurement systems have also shown to be proportional to the magnitude of the value measured for all three parameters assessed, as indicated by the regression equations (see figure 2A, 2C, 2E) and the slope of the regression lines in Bland–Altman plots (see figure 2B, 2D, 2F) [21]. Therefore, lower absolute bias is to be expected when the magnitude of applied V_{rep} , F_{rep} or P_{rep} are low.

One limitation of this study is that measurements have been exclusively registered from one inertial training system (“YoYo squat” – YoYo Technology, Stockholm, Sweden). Therefore, the extrapolation of the results to substantially different systems (i.e. conic pulleys) is limited. Another aspect to take into account is that the diameter of the axis of the system used was slightly variable across the range of motion, depending on the winding up of the strap (i.e. as the strap winds up over deeper layers of the strap, the diameter increases). Therefore, the mean diameter of the axis was used for the calculations. As this fact may have contributed to increasing the error of measurement, it is to be expected better accuracy in other inertial systems in which axis diameter remains constant throughout the repetition.

Despite the existence of other valid methods to monitor velocity, force and power in flywheel devices [9, 10], to our knowledge currently there are no other low-cost tools that work with free, open-code software to monitor a wide variety of flywheel resistance exercises. Given the practicality (e.g. minimal set-up), versatility (e.g. applicable to multiple systems and configurations) and cost of this sensor compared with other available options, practitioners may prefer this method for assessing V_{rep} , F_{rep} and P_{rep} in flywheel exercises.

CONCLUSIONS

In the last years, there has been a growing interest in flywheel resistance training [22]. Research in this area has shown greater increases in power and force with flywheel training [6, 23–25], improvements in changes of directions [26, 27] and other kinematics responses [28, 29], early hypertrophic adaptations [14] and changes in movement variability with functional resistance training exercises [30]. Nonetheless, only a few works have investigated the accuracy of rotary encoders for monitoring flywheel resistance training [9, 10, 13], and none had validated the use of rotary friction encoders, which can be adapted to different inertial training systems.

Inasmuch as the importance of the use of feedback [20, 31] and the control of velocity loss [32, 33] in resistance training using free weights, the validation of this rotary friction encoder and his open-code software could help strength and conditioning coaches to confidently monitor force, power and velocity in any flywheel machine, and therefore improve the control of training whenever using these resistance training devices, both with low and high training loads.

Coaches and sports scientists may confidently use a Chronojump friction encoder for assessing velocity, force and power in flywheel exercises, allowing for a simplified, accurate and versatile way of testing and monitoring athletes daily.

Acknowledgements

The authors would like to thank the volunteers who participated in the study. This research was funded by:

- FUNDACIÓ TECNOCAMPUS MATARÓ-MARESME,
- INEFC;
- AGAUR (2017SGR741);
- MICINN (DEP2016–8085-R);
- ESA (12RL000214);
- and MECD (FPU14/03006 and FPU15/03235).

Conflict of interest declaration

The authors declare no conflict of interest.

REFERENCES

1. Gabbett TJ, Nassis GP, Oetter E, Pretorius J, Johnston N, Medina D, Rodas G, Myslinski T, Howells D, Beard A, Ryan A. The athlete monitoring cycle: a practical guide to interpreting and applying training monitoring data. *Br J Sports Med.* 2017; 51:1451–2.
2. Bourdon PC, Cardinale M, Murray A, Gastin P, Kellmann M, Varley MC, Gabbett TJ, Coutts AJ, Burgess DJ, Gregson W. Monitoring Athlete Training Loads: Consensus Statement. *Int J Sports Physiol Perform.* 2017; 12(s2):161–70.
3. Scott BR, Duthie GM, Thornton HR, Dascombe BJ. Training Monitoring for Resistance Exercise: Theory and Applications. *Sports Medicine.* 2016; 46(5):687–98.
4. Berg HE, Tesch PA. Force and power characteristics of a resistive exercise device for use in space. *Acta Astronaut.* 1998; 42(1–8):219–30.
5. Petré H, Wernstål F, Mattsson CM. Effects of Flywheel Training on Strength-Related Variables: a Meta-analysis. *Sports Med Open.* 2018; 4(1):55.
6. Maroto-Izquierdo S, García-López D, Fernandez-Gonzalo R, Moreira OC, González-Gallego J, de Paz JA. Skeletal muscle functional and structural adaptations after eccentric overload flywheel resistance training: a systematic review and meta-analysis. *J Sci Med Sport.* 2017; 20(10):943–51.
7. Muñoz-López A, de Souza Fonseca F, Ramírez-Campillo R, Gantois P, Nuñez FJ, Nakamura FY. The use of real-time monitoring during flywheel resistance training programmes: how can we measure eccentric overload? A systematic review and meta-analysis. *Biol Sport.* 2021; 38(4):639–52.
8. Pérez-Castilla A, Piepoli A, Delgado-García G, Garrido-Blanca G, García-Ramos A. Reliability and Concurrent Validity of Seven Commercially Available Devices for the Assessment of Movement Velocity at Different Intensities During the Bench Press. *J Strength Cond Res.* 2019 May; 33(5):1258–65.
9. Weakley J, Fernández-Valdés B, Thomas L, Ramirez-Lopez C, Jones B. Criterion Validity of Force and Power Outputs for a Commonly Used Flywheel Resistance Training Device and Bluetooth App. *J Strength Cond Res.* 2019 May; 33(5):1180–4.
10. Martín-San Agustín R, Sánchez-Barbadora M, García-Vidal JA. Validity of an inertial system for measuring velocity, force, and power during hamstring exercises performed on a flywheel resistance training device. *PeerJ.* 2020; 8:e10169.
11. Vázquez-Guerrero J, Moras G, Baeza J, Rodríguez-Jiménez S. Force outputs during squats performed using a rotational inertia device under stable versus unstable conditions with different loads. *PLoS One.* 2016; 11(4):1–13.
12. Tous-fajardo J, Maldonado RA, Quintana JM, Pozzo M, Tesch PA. The Flywheel Leg-Curl Machine: Offering Eccentric Overload for Hamstring Development. *Int J Sports Physiol Perform.* 2006; 1(3):293–8.
13. Bollinger LM, Brantley JT, Tarlton JK, Baker PA, Seay RF, Abel MG. Construct Validity, Test-Retest Reliability, and Repeatability of Performance Variables Using a Flywheel Resistance Training Device. *J Strength Cond Res.* 2020; 34(11):3149–56.
14. Illera-Domínguez V, Nuell S, Carmona G, Padullés JM, Padullés X, Lloret M, Cussó R, Alomar X, Cadefau JA. Early Functional and Morphological Muscle Adaptations During Short-Term Inertial-Squat Training. Vol. 9, *Frontiers in Physiology.* 2018. p. 1265.
15. Sabido R, Pombero L, Hernández-Davó JL. Differential effects of low vs high inertial loads during an eccentric-overload training intervention in rugby union players: a preliminary study. *J Sports Med Phys Fitness.* 2019; 59(11):1805–11.
16. Chronojump. Chronojump open code repository [Internet]. 2014 [cited 2019 Nov 15]. Available from: <https://git.gnome.org/browse/chronojump/>
17. Hopkins W. Spreadsheets for analysis of validity and reliability. *Sportscience* [Internet]. 2015; 19:36–42. Available from: [sportsci.org/2015/ValidRely.htm](https://www.sportsci.org/2015/ValidRely.htm)
18. Martin Bland J, Altman DG. Statistical methods for assessing agreement between two methods of clinical measurement. *The Lancet.* 1986 Feb 8; 327(8476):307–10.
19. Bautista IJ, Chiroso IJ, Robinson JE, Chiroso LJ, Martínez I. Concurrent Validity of a Velocity Perception Scale to Monitor Back Squat Exercise Intensity in Young Skiers. *J Strength Cond Res.* 2016; 30(2):421–9.
20. Weakley J, Wilson K, Till K, Banyard H, Dyson J, Phibbs P, Read D, Jones B. Show Me, Tell Me, Encourage Me: The Effect of Different Forms of Feedback on Resistance Training Performance. *J Strength Cond Res.* 2018; 34(11):3157–63.

21. Giavarina D. Understanding bland altman analysis. *Biochem Med (Zagreb)*. 2015; 25(2):141–51.
22. de Keijzer K, McErlain-Naylor SA, Brownlee TE, Raya-González J, Beato M. Perception and application of flywheel training by professional soccer practitioners. *Biol Sport*. 2022; 39(4):809–17.
23. Norrbrand L, Pozzo M, Tesch PA. Flywheel resistance training calls for greater eccentric muscle activation than weight training. *Eur J Appl Physiol*. 2010; 110(5):997–1005.
24. Martínez-Aranda LM, Fernández-Gonzalo R. Effects of Inertial Setting on Power, Force, Work, and Eccentric Overload During Flywheel Resistance Exercise in Women and Men. *J Strength Cond Res*. 2017; 31(6):1653–61.
25. Vicens-Bordas J, Esteve E, Fort-Vanmeerhaeghe A, Bandholm T, Thorborg K. Is inertial flywheel resistance training superior to gravity-dependent resistance training in improving muscle strength? A systematic review with meta-analyses. *J Sci Med Sport*. 2018; 21(1):75–83.
26. Tous-Fajardo J, Gonzalo-Skok O, Arjol-Serrano JL, Tesch PA. Enhancing change-of-direction speed in soccer players by functional inertial eccentric overload and vibration training. *Int J Sports Physiol Perform*. 2016; 11(1):66–73.
27. De Hoyo M, De La Torre A, Pradas F, Sañudo B, Carrasco L, Mateo-Cortes J, Domínguez-Cobo S, Fernandes O, Gonzalo-Skok O. Effects of eccentric overload bout on change of direction and performance in soccer players. *Int J Sports Med*. 2015; 36(04):308–14.
28. de Hoyo M, Pozzo M, Sanudo B, Carrasco L, Gonzalo-Skok O, Domínguez-Cobo S, Moran-Camacho E. Effects of a 10-week in-season eccentric-overload training program on muscle-injury prevention and performance in junior elite soccer players. *Int J Sports Physiol Perform*. 2014/06/10. 2015; 10(1):46–52.
29. Gonzalo-Skok O, Tous-Fajardo J, Arjol-Serrano JL, Suarez-Arrones L, Casajús JA, Mendez-Villanueva A. Improvement of Repeated-Sprint Ability and Horizontal-Jumping Performance in Elite Young Basketball Players With Low-Volume Repeated-Maximal-Power Training. *Int J Sports Physiol Perform*. 2016; 11(4):464–73.
30. Moras G, Fernández-Valdés B, Vázquez-Guerrero J, Tous-Fajardo J, Exel J, Sampaio J. Entropy measures detect increased movement variability in resistance training when elite rugby players use the ball. *J Sci Med Sport*. 2018; 21(12):1286–92.
31. Weakley J, Wilson KM, Till K, Read DB, Darrall-Jones J, Roe G, Phibbs PJ, Jones B. Visual feedback attenuates mean concentric barbell velocity loss, and improves motivation, competitiveness, and perceived workload in male adolescent athletes. *J Strength Cond Res*. 2017 Jul; 33(9):2420–5.
32. Sánchez-Medina L, González-Badillo JJ. Velocity Loss as an Indicator of Neuromuscular Fatigue during Resistance Training. *Med Sci Sports Exerc*. 2011; 43(9):1725–34.
33. Pareja-Blanco F, Rodríguez-Rosell D, Sánchez-Medina L, Gorostiaga EM, González-Badillo JJ. Effect of movement velocity during resistance training on neuromuscular performance. *Int J Sports Med*. 2014; 35(11):916–24.